

Purpose and Objective –scintillator array solution to dynamic IVD

On-patient dosimeters assist in clinical decision-making by measuring surface dose, but single-point measurements cannot monitor area-wide distributions and are misleading in high-gradient regions. In breast radiotherapy, steep dose gradients and complex surface contours can increase contralateral breast dose and, consequently, increase the risk of secondary malignancy. **This work introduces a 2.5D surface dosimetry technique using a wide-area deformable scintillator array combined with Cherenkov imaging for regional dose monitoring in high-gradient areas.**

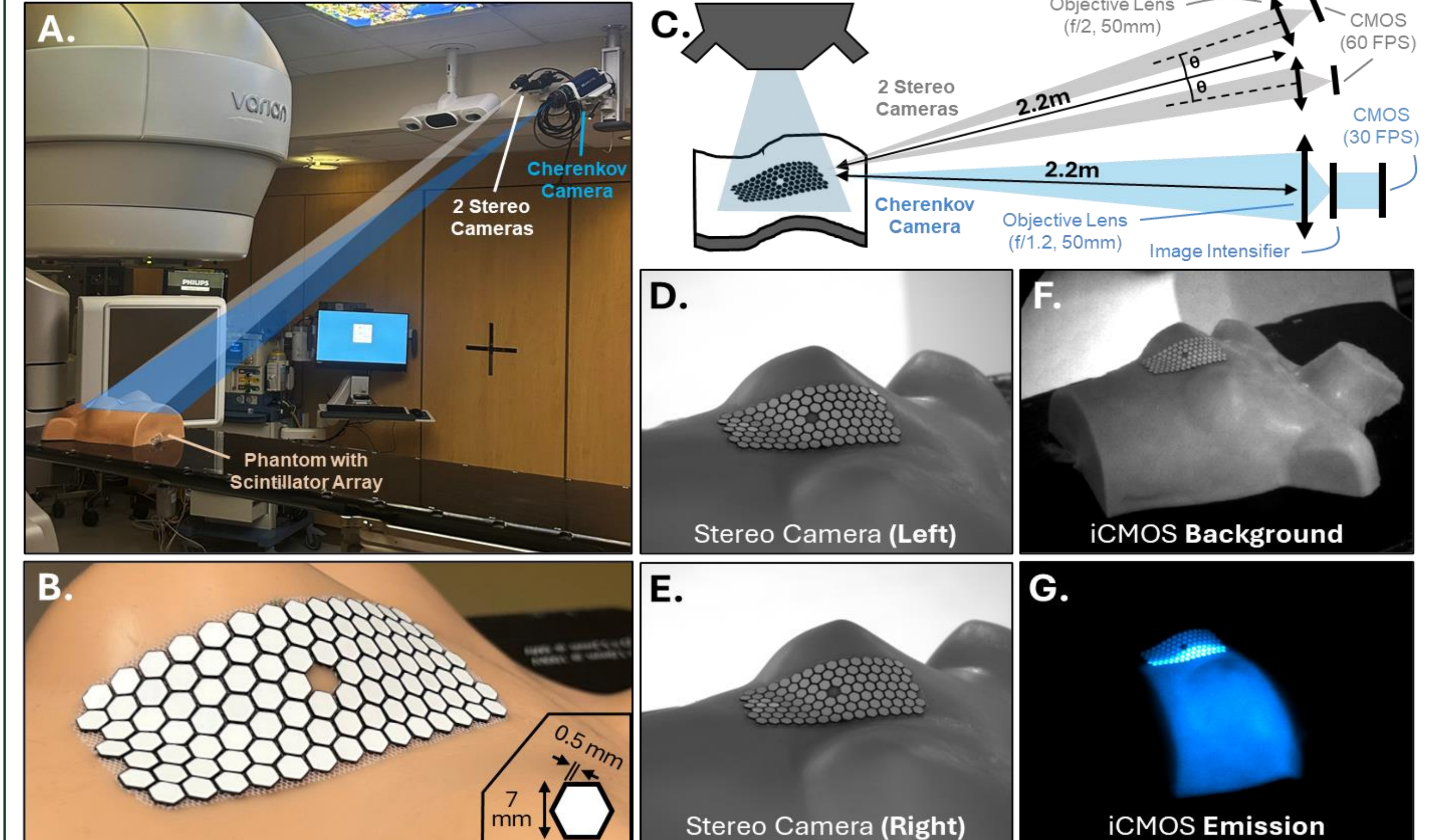


Figure 1: (a) Dual-stereovision system setup mounted adjacent to clinical Cherenkov camera. (b) A detailed view of the scintillator array on an anthropomorphic phantom. (c) A diagram of the imaging setup is highlighted and sample image outputs from the stereovision modules (d-e) and Cherenkov camera (f-g) are shown.

Method – 3D localization and angular correction via stereovision

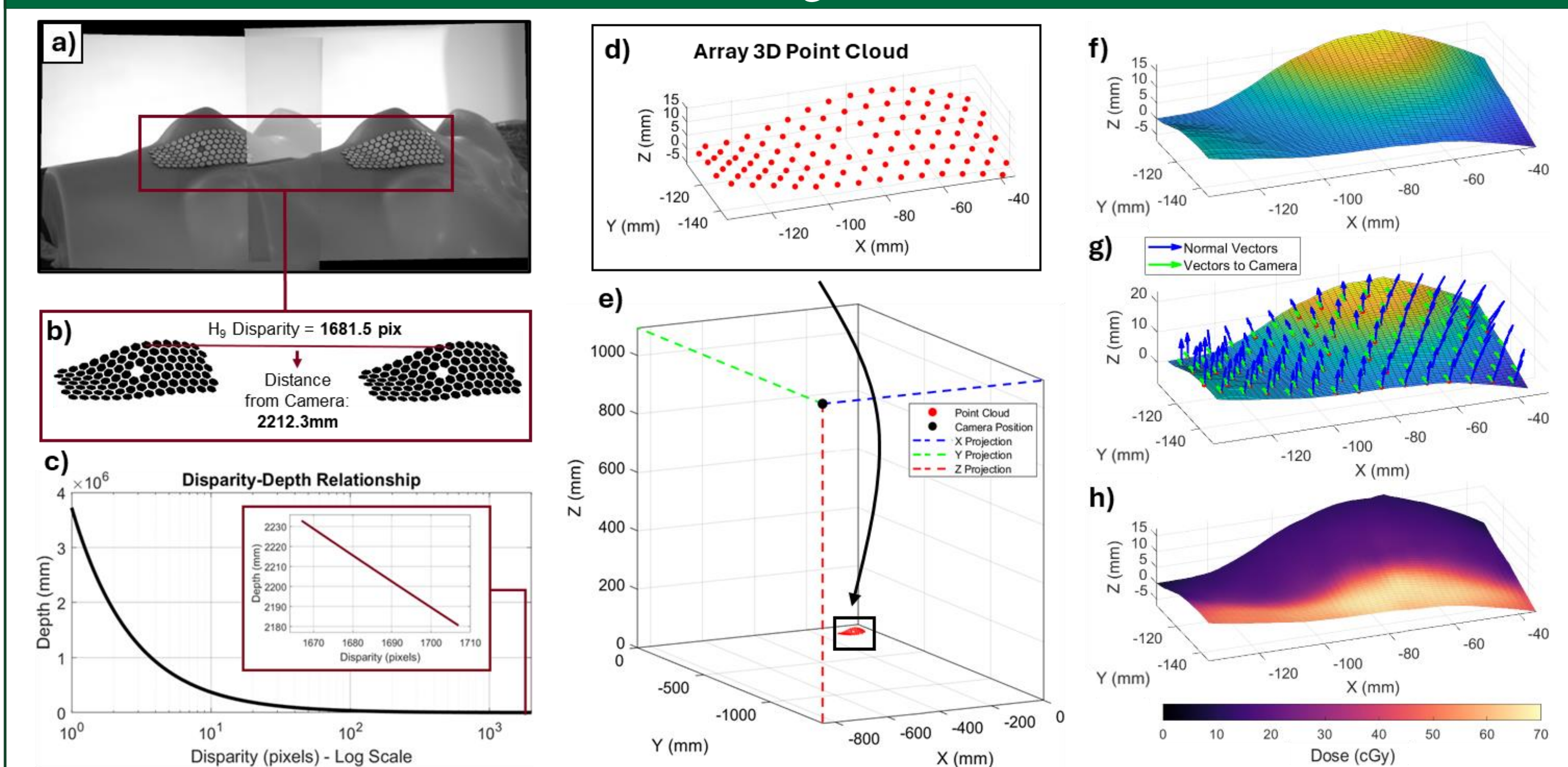


Figure 2: (a) Rectified image pair, (b) sample disparity definition using masked array profiles, (c) analytically derived relationship between disparity and depth, (d) sample array point cloud oriented in (e) the bunker environment with respect to the isocenter and the camera. (f) Interpolated surface with (g) normal and camera directional vectors, and a (h) sample dose map following angular correction and interpolation.

Results

Scintillator intensity demonstrated linearity with dose ($R^2 > 0.999$), remained within 5% for varying pulse repetition rates, and maintained minimal response deviation up to a camera angle of 50° . Stereovision positioning localized the 3D target surface in patient coordinates with 0.5mm accuracy. The system resolved continuous dose gradients up to 150cGy/cm at the field edge and captured real-time in vivo surface dose distributions during treatment revealing contralateral breast dose ranging from 230 cGy to 40 cGy. Across all deliveries, central TLDs agreed within 1% (1.5 cGy) of the interpolated dose map. Edge TLD deviations were higher due to extrapolation but still agreed within 20 cGy and 2 mm.

Clinical Translation – Scintillator array used to monitor contralateral breast dose in vivo

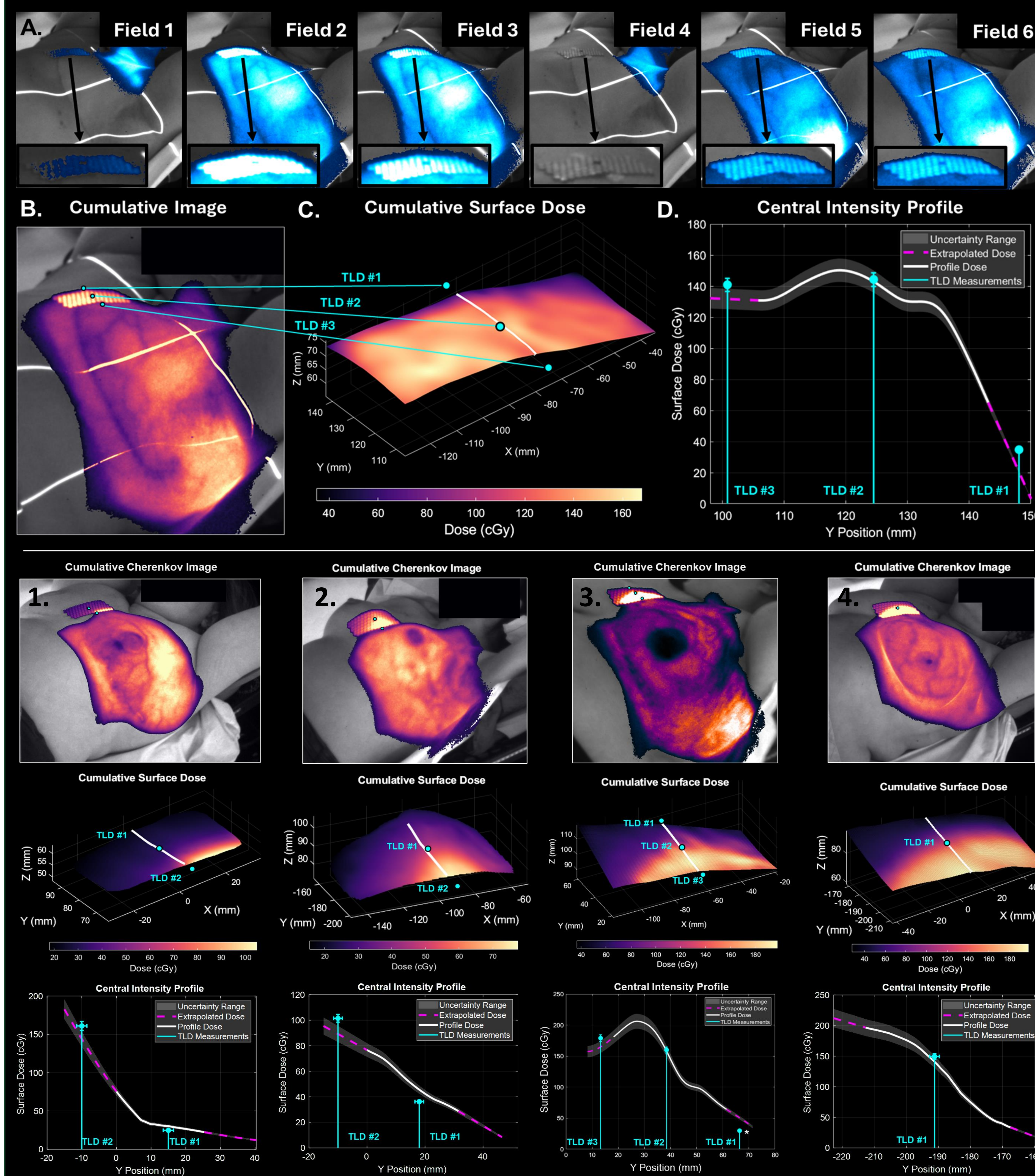


Figure 3: Single full process is highlighted (top) - scintillator array used to measure dose during a 6 field post-mastectomy radiotherapy treatment. (a) Signal from each field was isolated, localized, and corrected into a (b) cumulative image with 3 TLD measurements along the central axis of the array. Cumulative surface dose (c) was sampled along TLD path showing agreement within uncertainty (d). Resulting data from 4 additional patients is shown (1-4) highlighting cumulative Cherenkov, surface dose map, and central intensity comparison to TLDs.

Conclusions / Future Work

This work presents a time resolved 2.5D surface dosimetry method optimized for irregular surface geometry. This approach enables quantitative spatially-resolved dose measurements across non-uniform and high gradient treatment regions and clinical translation is ongoing.

Performance Analysis – Dose Linearity, Angular Characterization, Beam Impact

Current standard-of-care treatments leverage angular variation during delivery to optimize dose target coverage. Surface dosimetry has been shown to display significant dependence on irradiation angle, with up to 50% variation in emission compared to en-face delivery. Optical dosimeters exhibit additional dependence of emission intensity with angle to the imaging plane. **This work presents extensive characterization of scintillation emission variation with gantry angle and camera angle, linearity with dose, repetition rate, and build-up effect on the beam delivery.**

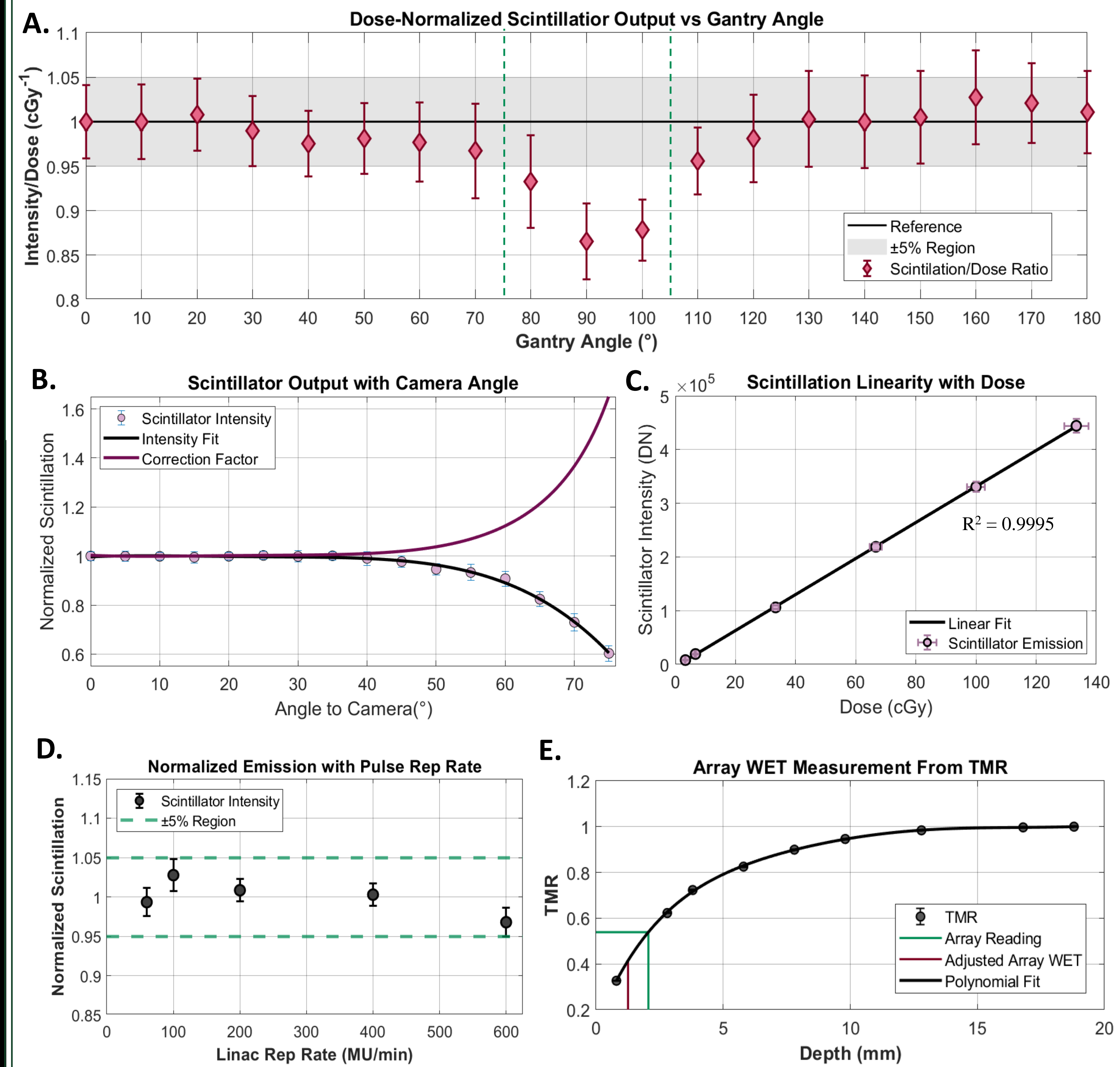


Figure 4: Scintillator variability with gantry angle is dose corrected and shown to remain within 5% in the region of interest for tangent treatments (a). (b) Scintillation emission and correction factors with camera angle are shown. (c) Scintillation response remains linear with dose ($R^2 = 0.9995$) for the range of interest (d) and remains within 5% deviation for varying pulse repetition rates. (e) Water equivalent thickness evaluation using TMR analysis indicates 1.1 mm array thickness.

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