

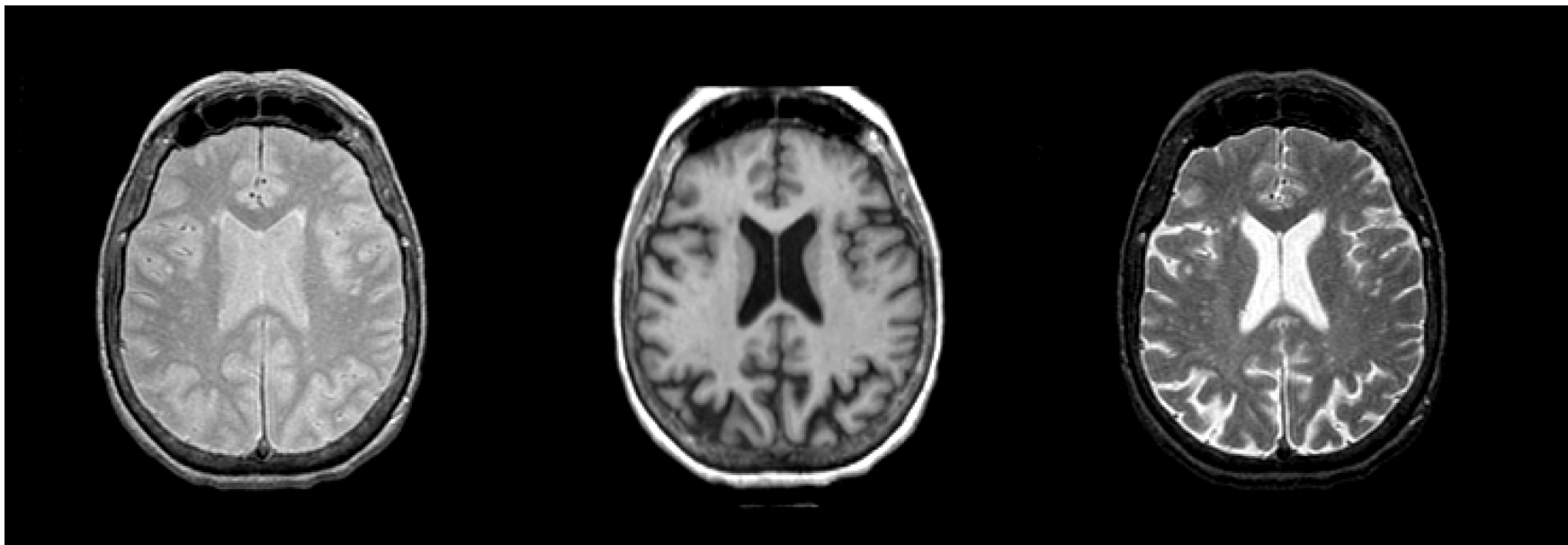
Introduction to NMR

Physical principles
Skejby Sept. 2003
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MRI of the human brain





Basic steps



- 1) By means of magnetic fields and RF pulses
- 2) Data processing (Fourier transformation)



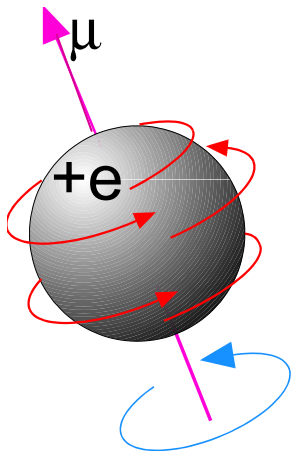
Outline

- Nuclear spins
- Spin dynamics in magnetic fields
- Spin interactions
- Spin excitation
- Spin RF radiation and detection

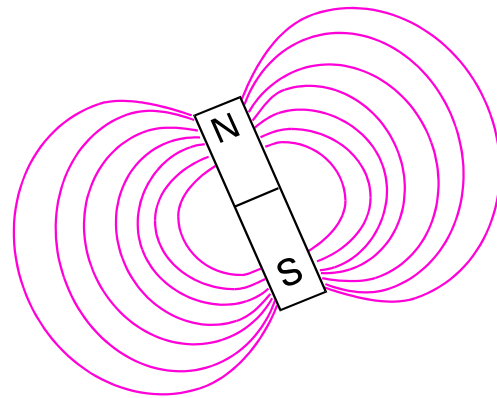


Spin and magnetic fields

Proton



Permanent
Magnet (dipole)



A charged proton that spins will create a circulating current which in turn induces a magnetic field.

The dipole vector μ describes the strength and direction of magnetic field. C.g. permanent magnet.

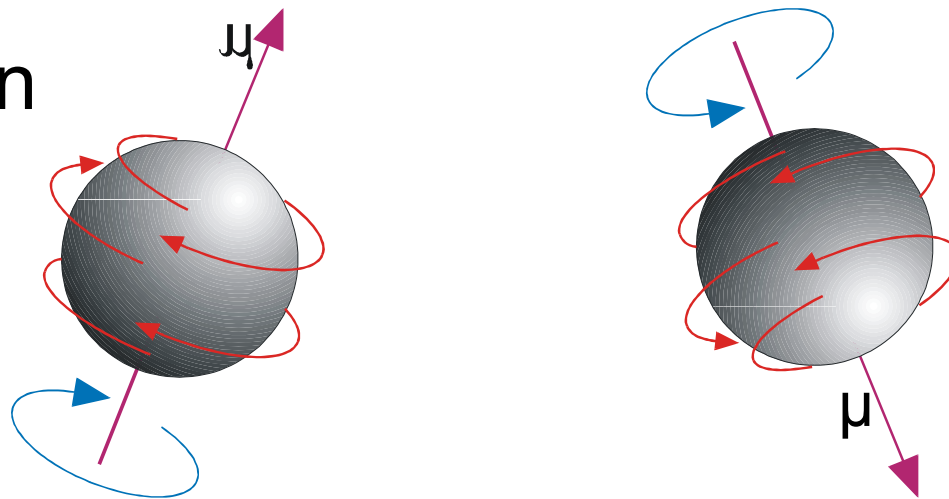


Spin is a fundamental quantum mechanical property. All nuclei (and other particles) have spin:

$S=0, 1/2, 1, 3/2, \dots \quad h/2\pi$ (Planck's constant).

For $S=I$ there are $2I+1$ states, corresponding to the possible orientations of the spin.

Proton





Spin and magnetic field

The fundamental

γ (gamma) is the
depends on the n
 $2,675 \cdot 10^8$ rad/s/T.

Only nuclei with non-zero spin have magnetic moments, and are thus NMR active.

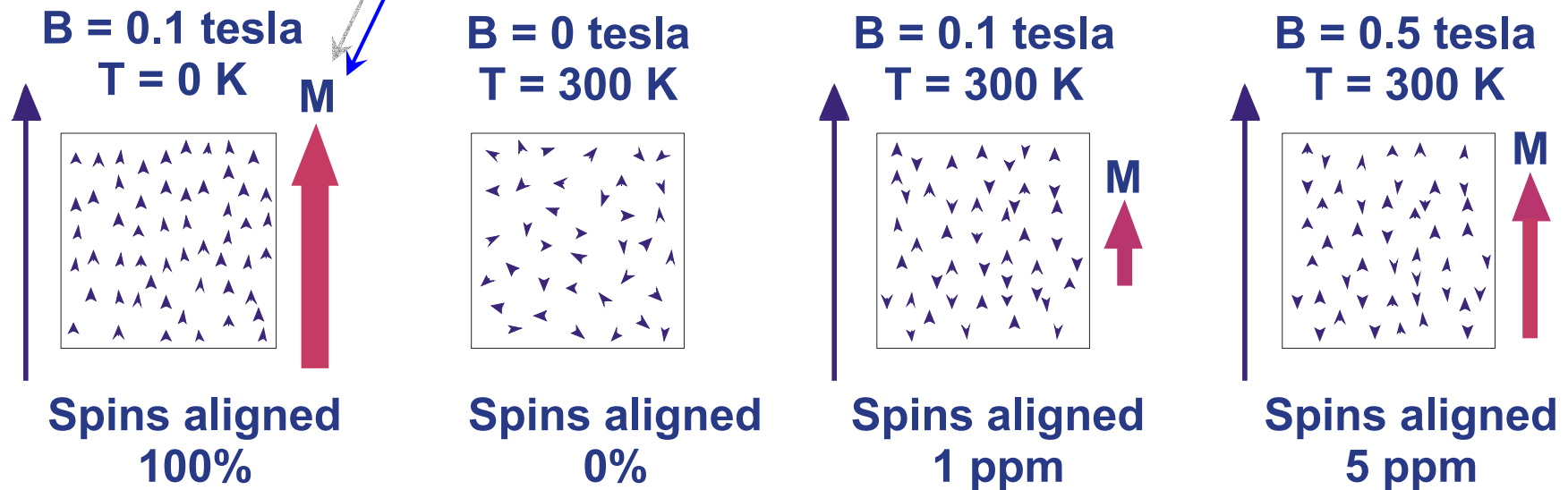
T=Tesla. 1 Gauss=10000
Tesla. Earths magnetic
field is roughly .5 Gauss.
A clinical scanner has 1.5
Tesla, i.e. 30000 times
the earths magnetic field.



Spins in external fields

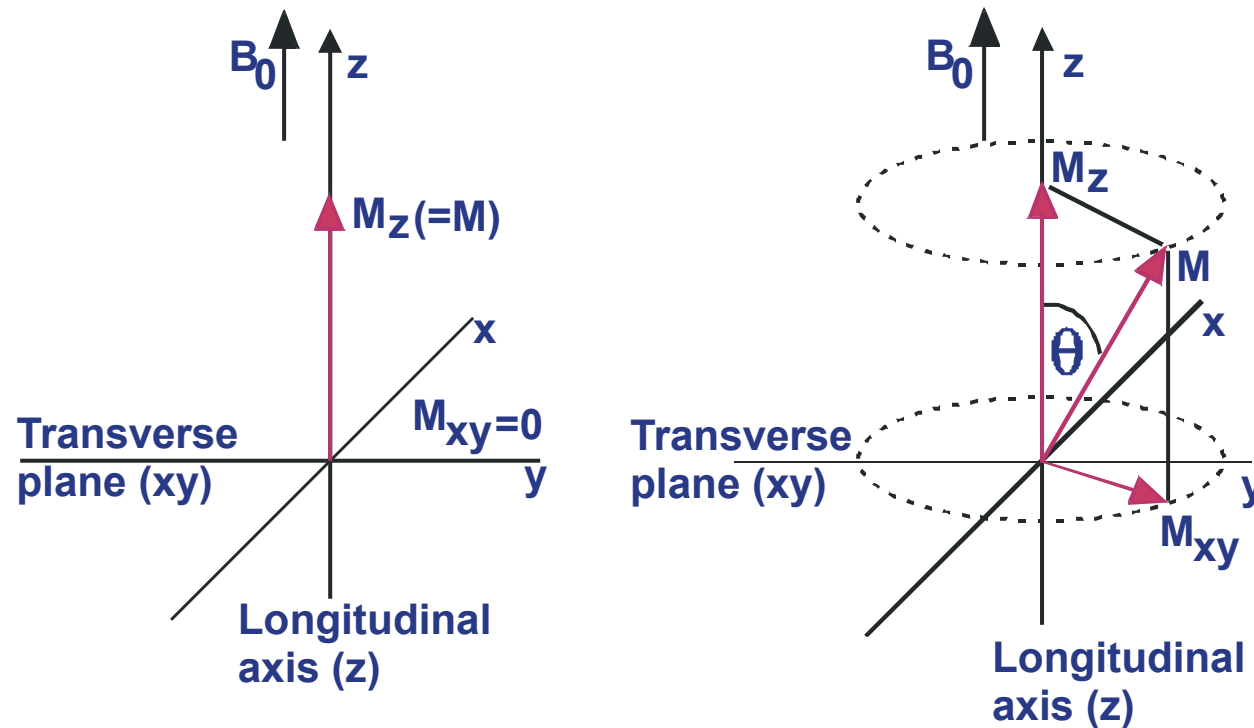
A magnetic dipole tends to align with an external field (e.g. a compass needle). Thermal motion opposes this.

M (magnetization) is the magnetic dipole moment per unit volume.



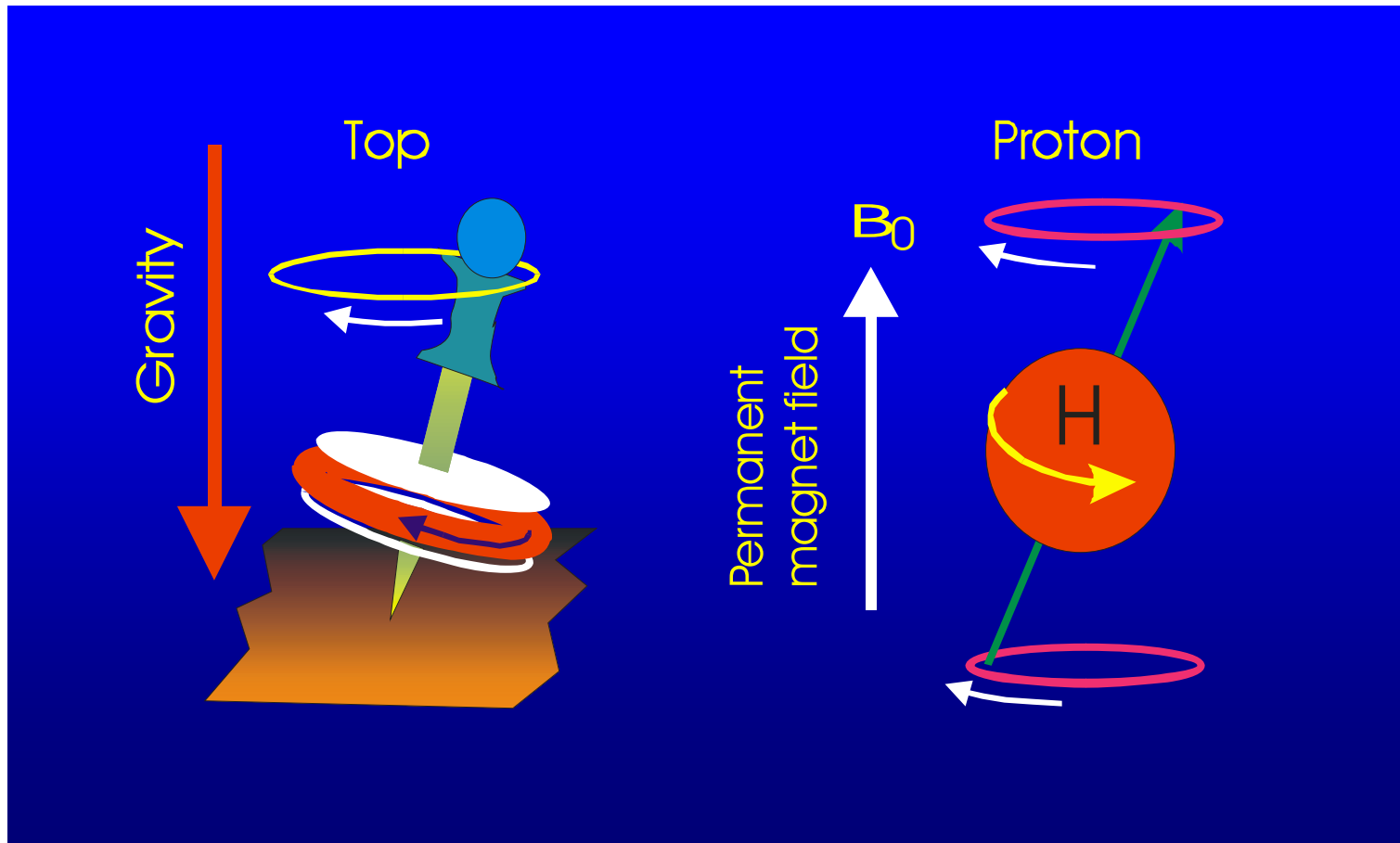


Magnetization



M is the sum of the individual spin magnetic moments.

Spin dynamics





Larmor frequency

ω is the Larmor frequency:

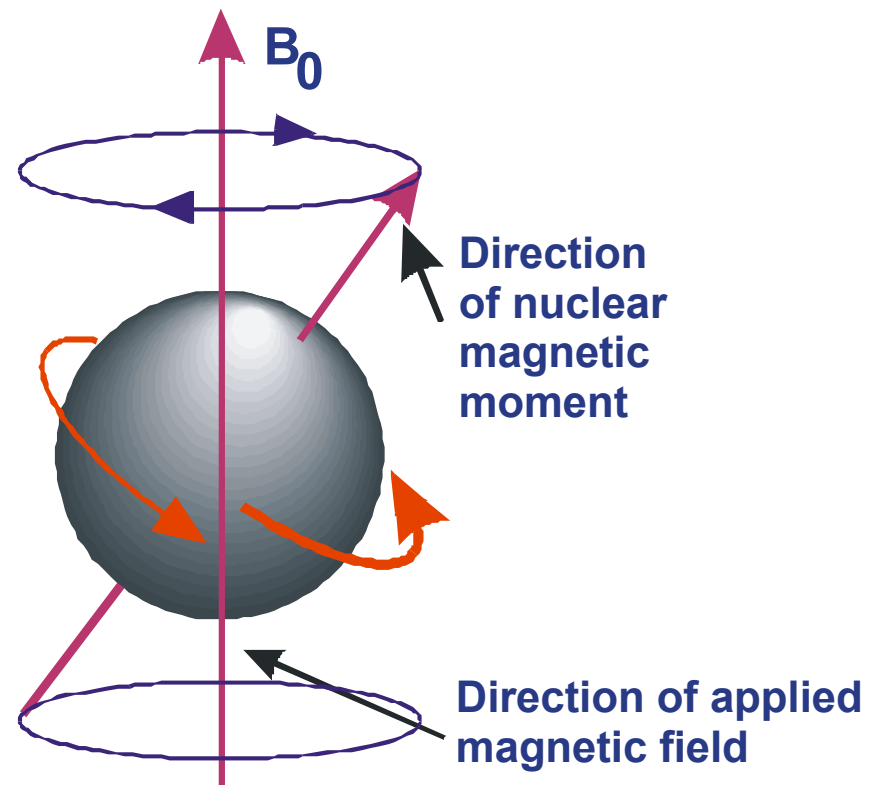
$$\omega_0 = \gamma B_0$$

For protons in a clinical scanner, $B_0 = 1.5\text{T}$ so

$$\omega_0 = 63.87\text{Mhz.}$$

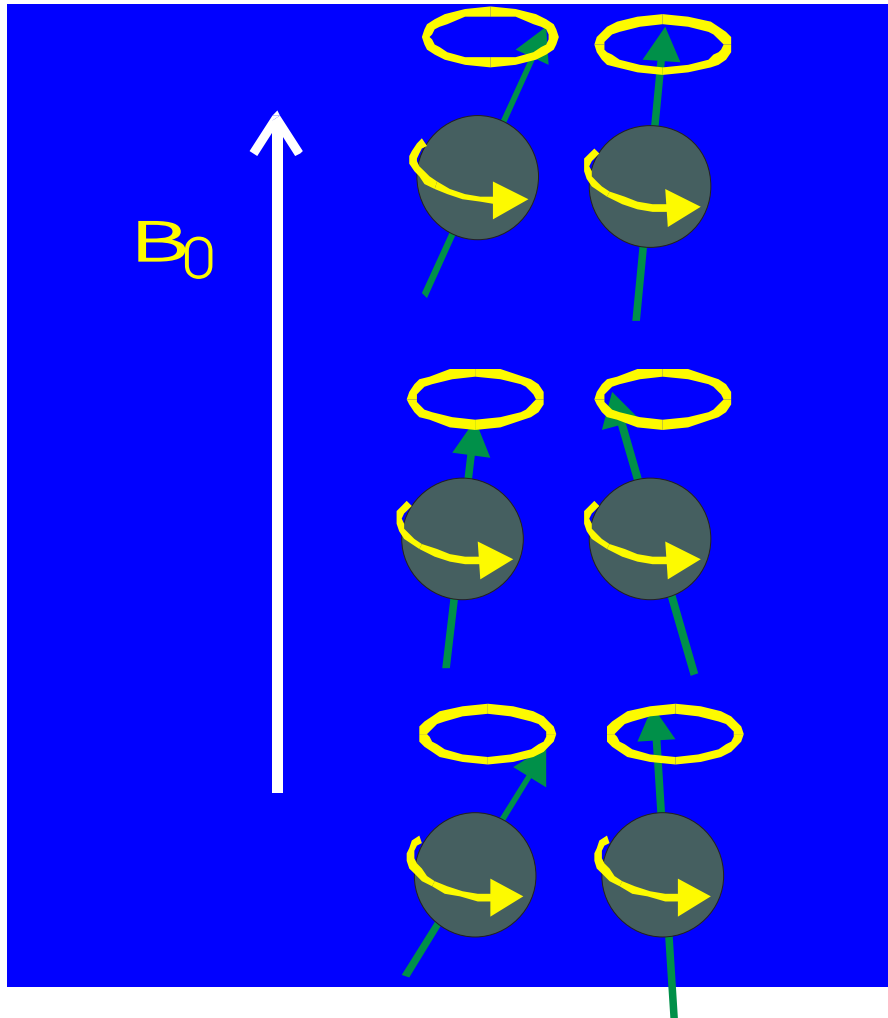
Compare

DRP1@88.1Mhz.





Magnetization



Magnetization M is:

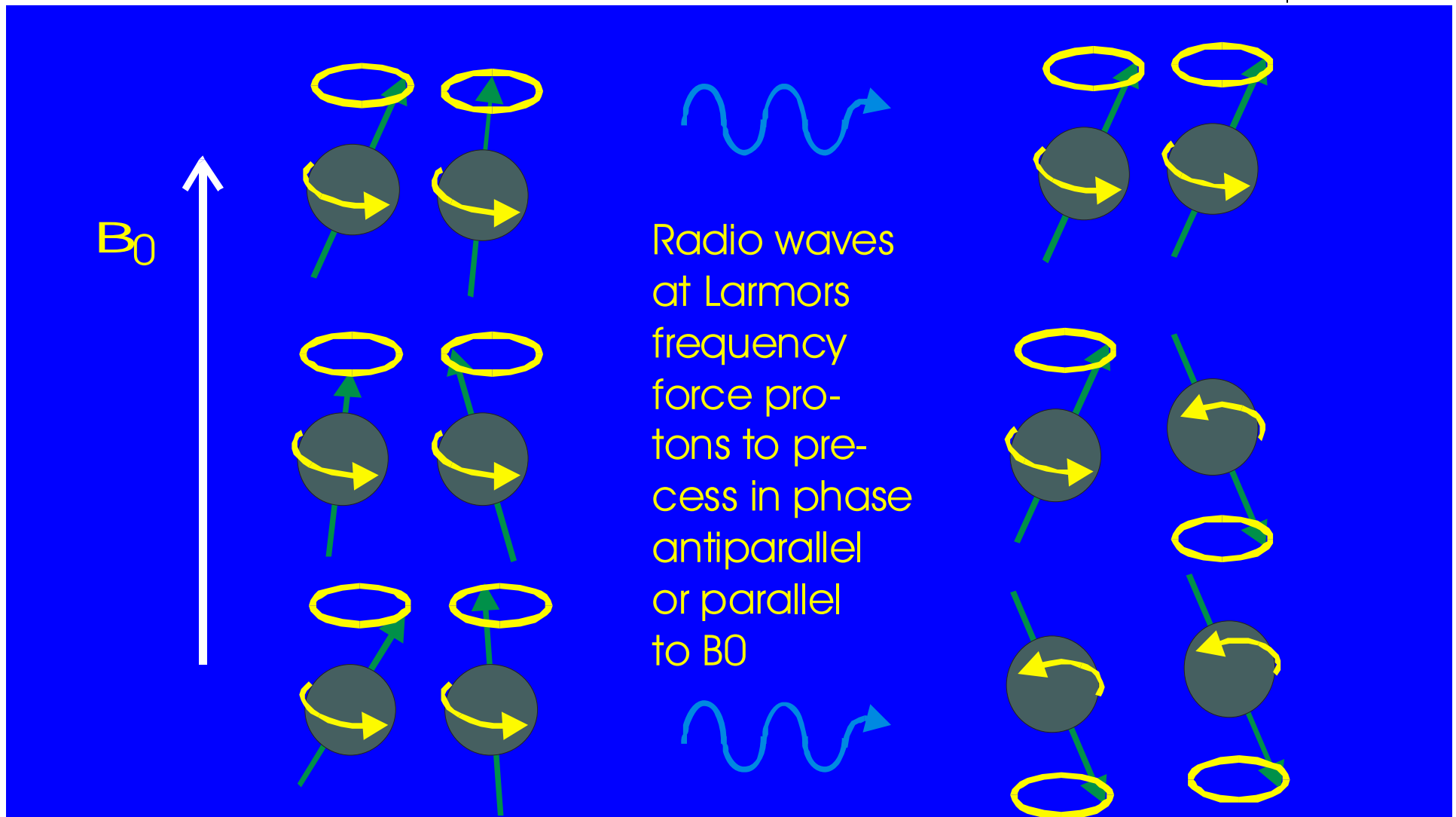
$$M_z = M_0$$

$$M_{xy} = 0$$

Transverse magnetization is zero because of random phases.

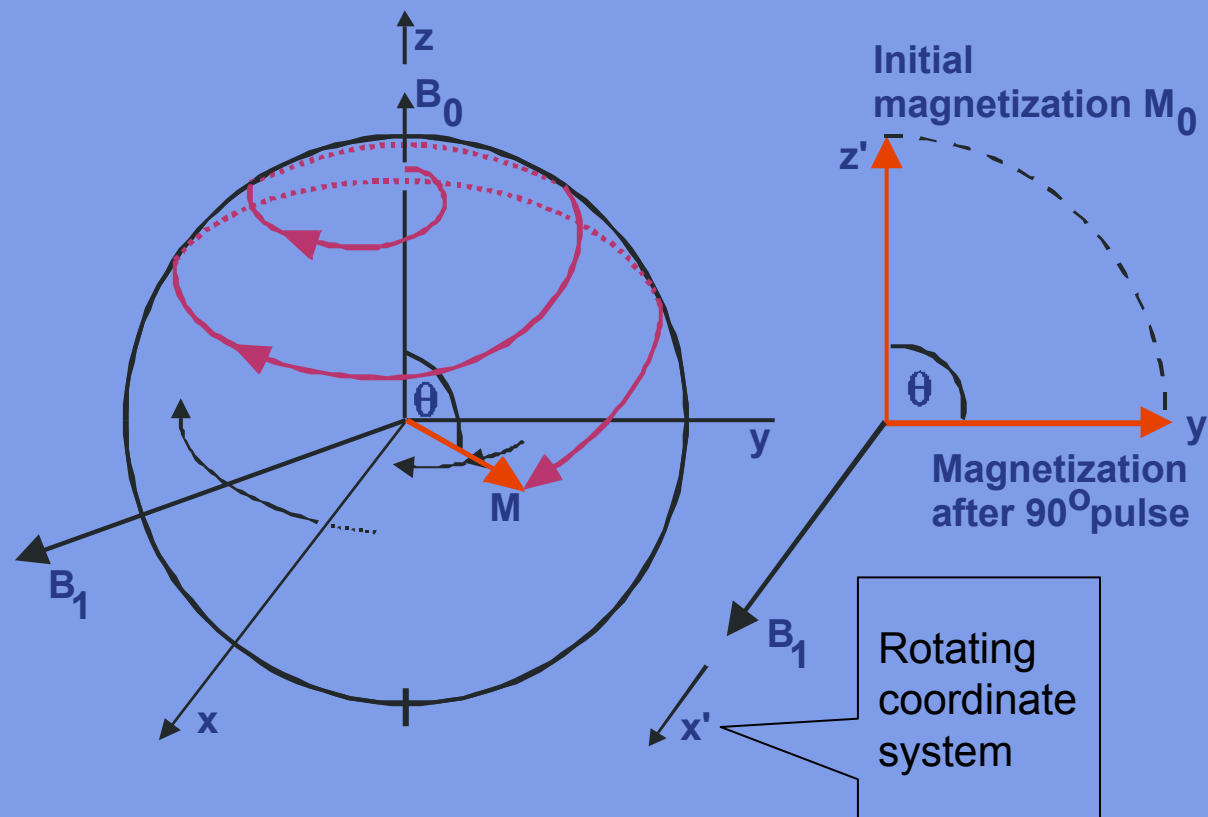


Radio-frequency pulses





RF pulses and magnetization

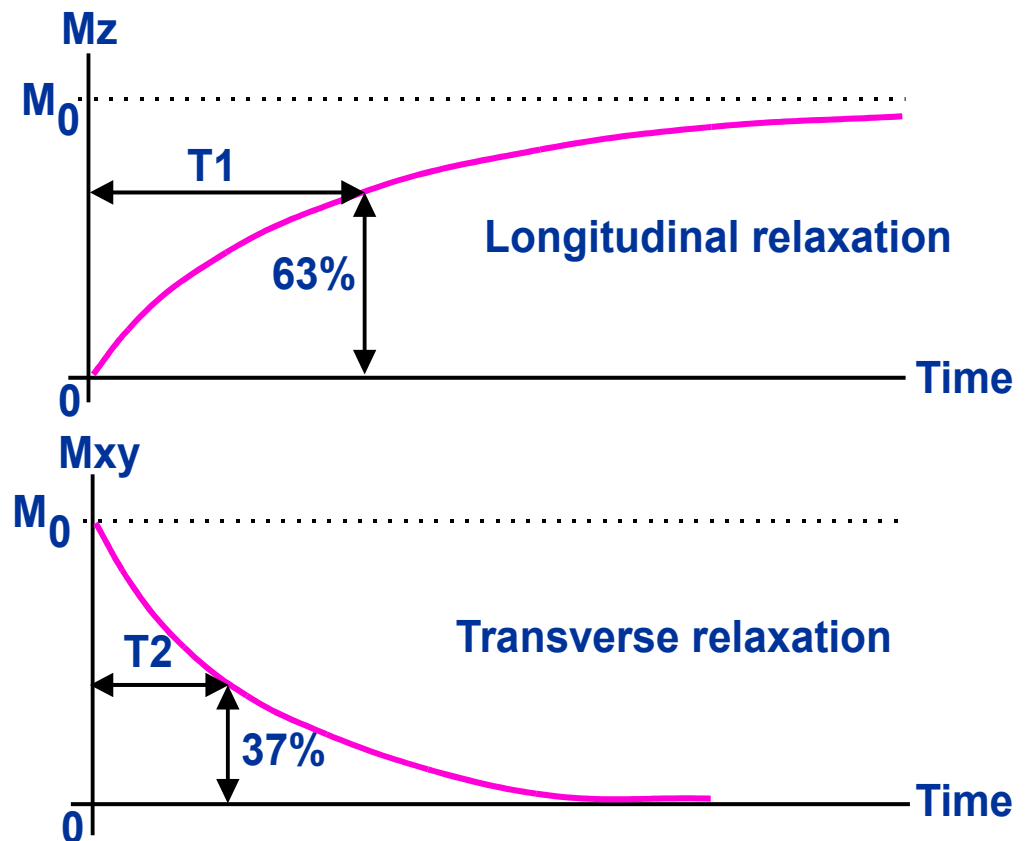




Spin interactions

Instead of precessing forever in the transverse plane, the magnetization relaxes back to the equilibrium value.

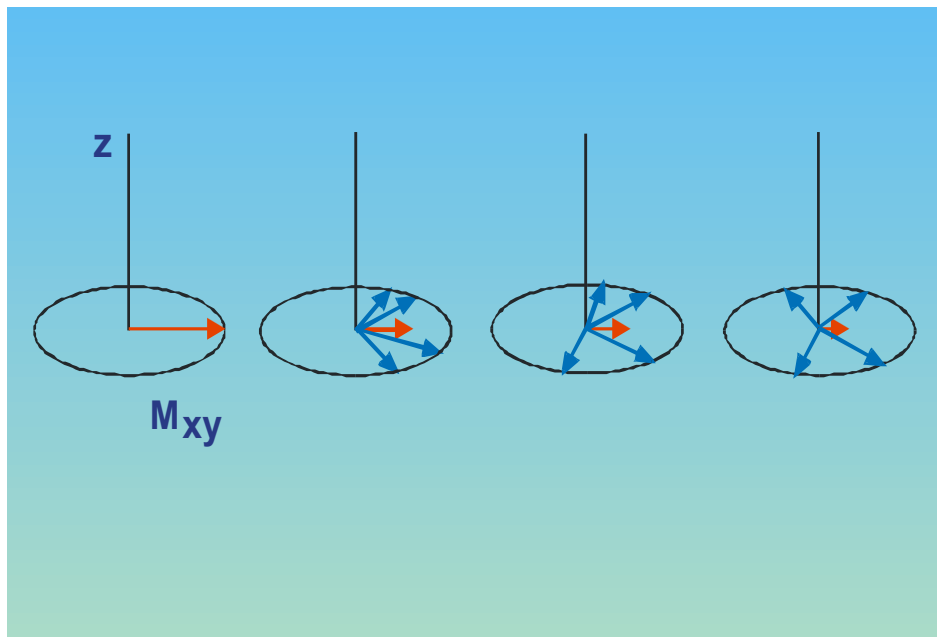
T1 and T2 are characteristic relaxation constants.





T2 and T2*

T2 dephasing



The dephasing in T2 relaxation results from differing local interactions, leading to locally varying Larmor frequencies. T2* is the same phenomenon, but is a result from magnetic field inhomogeneities.

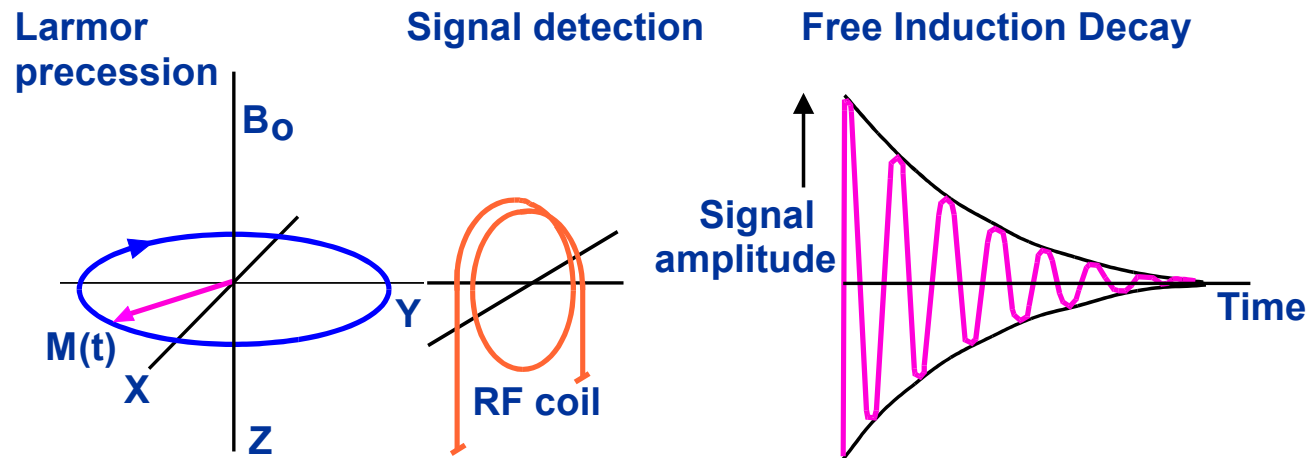


Biological T1-T2 values

<i>TISSUE</i>	<i>T1 at 1.5 T (ms)</i>	<i>T1 at 0.5 T (ms)</i>	<i>T2 (ms)</i>
<i>Skeletal muscle</i>	870	600	47
<i>Liver</i>	490	323	43
<i>Kidney</i>	650	449	58
<i>Spleen</i>	780	554	62
<i>Fat</i>	260	215	84
<i>Grey matter</i>	920	656	101
<i>White matter</i>	790	539	92
<i>Cerebrospinal fluid</i>	>4000	>4000	>2000
<i>Lung</i>	830	600	79



Spin RF radiation and detection



Law of induction: changing magnetic field induces electromotoric force. From M_{xy}

Detected by RF coil and measured as a time varying current. Decays according to T_2^* . What about T_2 ?

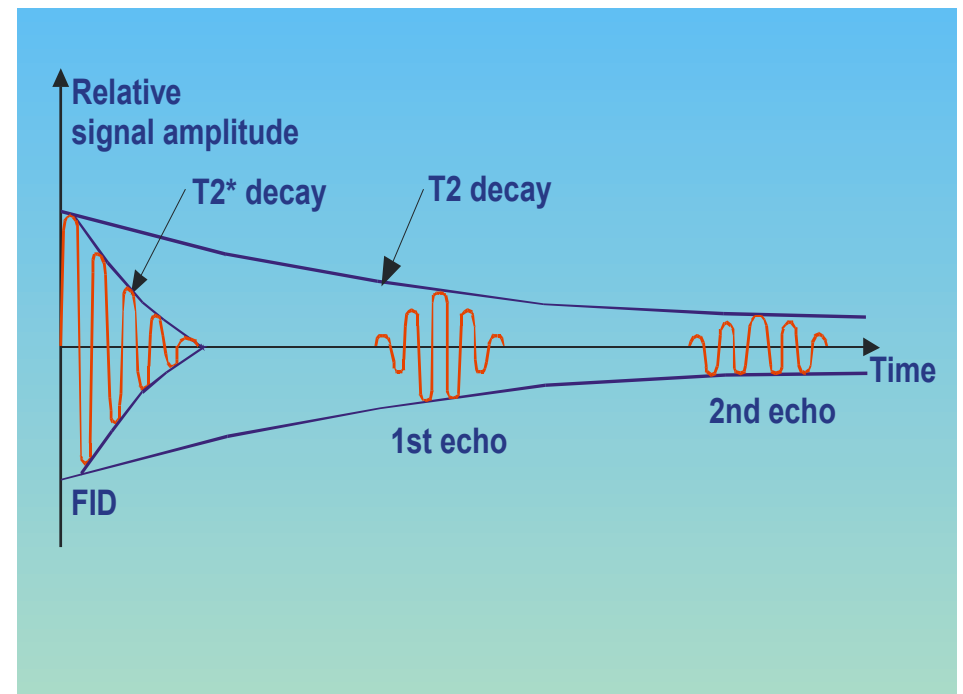
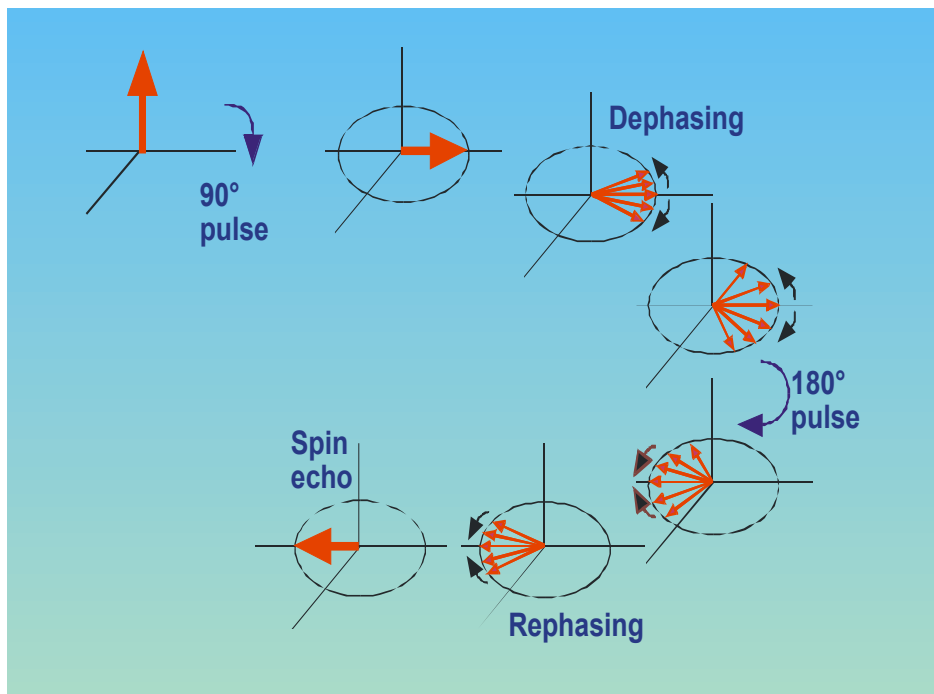
Spin echo





Spin echo

- Or spin refocussing



[90]-TE/2-[180]-TE/2-ECHO



Pulse sequences and contrast

By using different pulse sequences, one can create contrast on the basis of e.g. T1, T2, T2* or spin density.

Spin echo:

$$S = \rho \cdot (1 - e^{-TR/T_1}) \cdot e^{-TE/T_2}$$

Overview

Generation of a NMR-spectrum

